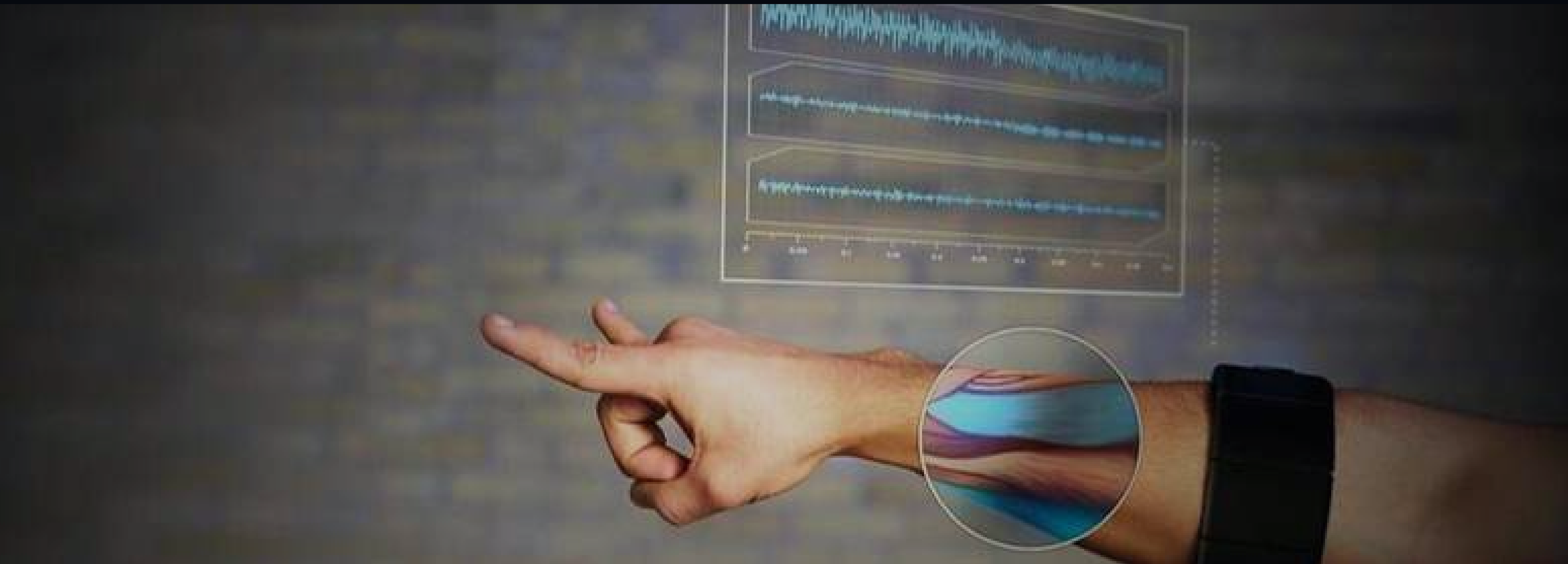


ADVANCING **HUMAN-MACHINE INTERFACE** SYSTEMS THROUGH ARTIFICIAL INTELLIGENCE



AUTHOR: SAMUEL GEORGE-WHITE
SUPERVISORS: ANIL BHARATH, DARIO FARINA

STEM
THINK
TANK

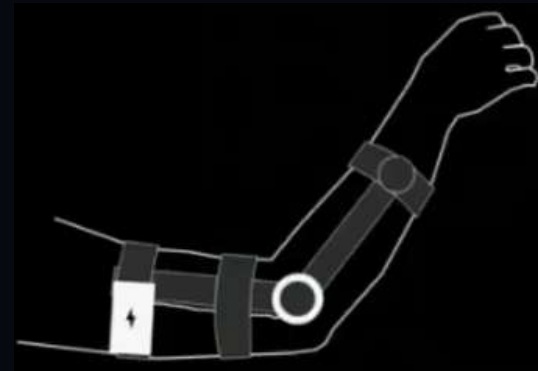
IMPERIAL

AUGMENTING HUMAN MOTOR CAPACITIES



A TAXONOMY OF MOVEMENT AUGMENTATION

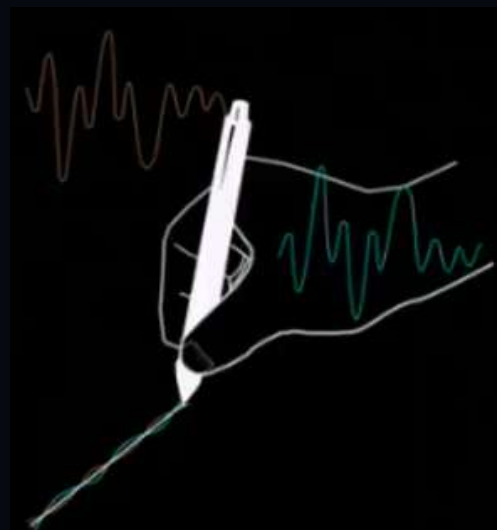
Power augmentation to increase the exertable forces or movement speed



Degrees-of-freedom augmentation increases the number of DoFs enabling users to perform more complex tasks than with the natural DoFs alone



Workstation augmentation to extend the spacial reach of natural limbs



Precision augmentation increases the control precision and task performance



Task



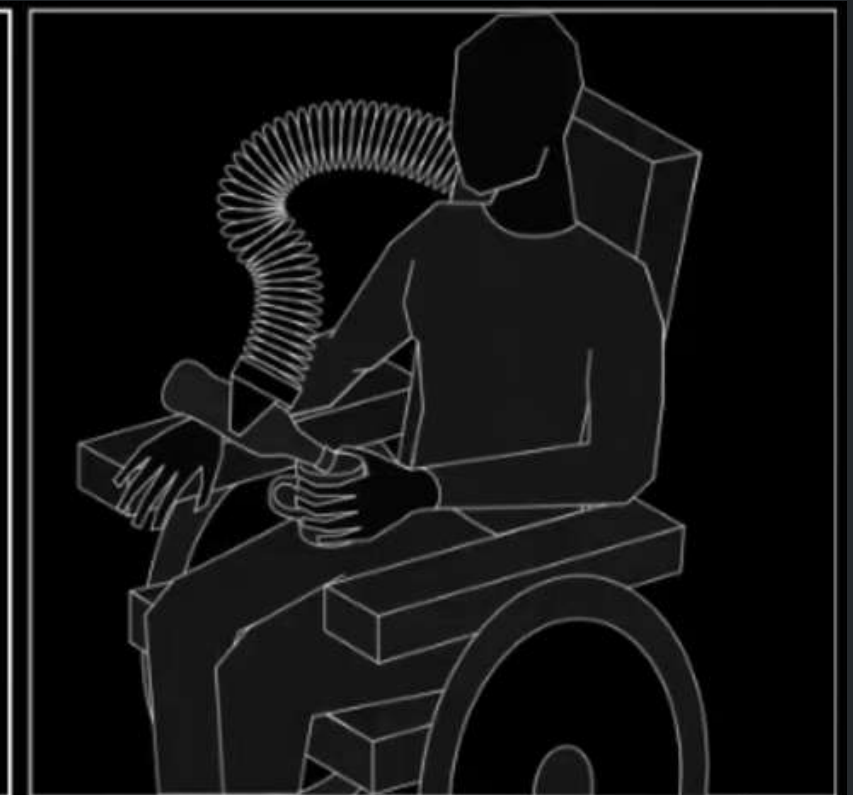
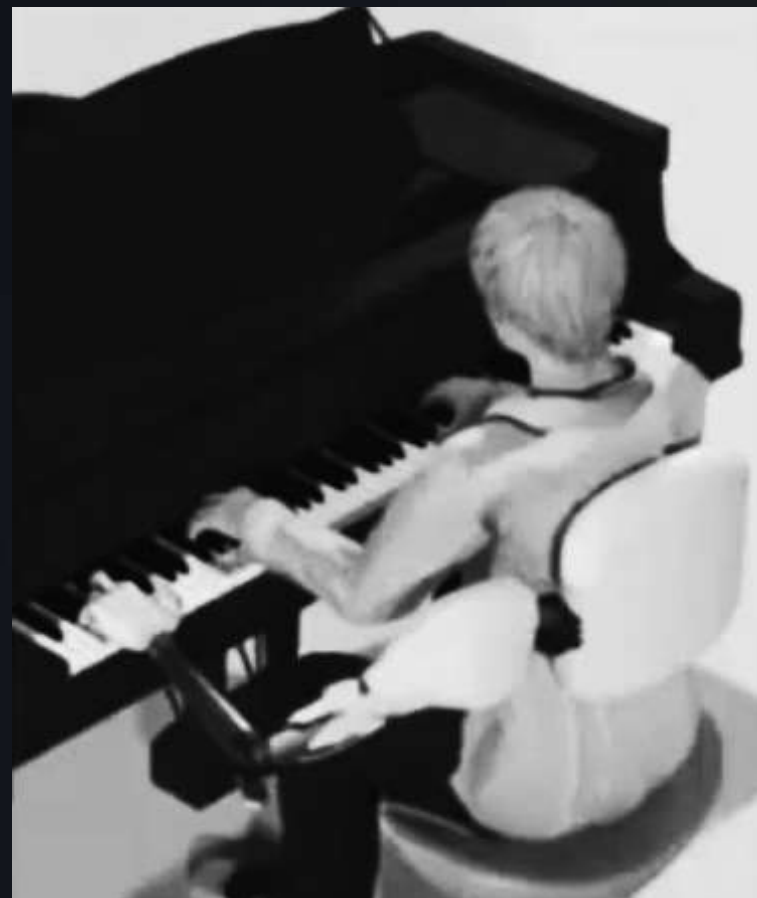
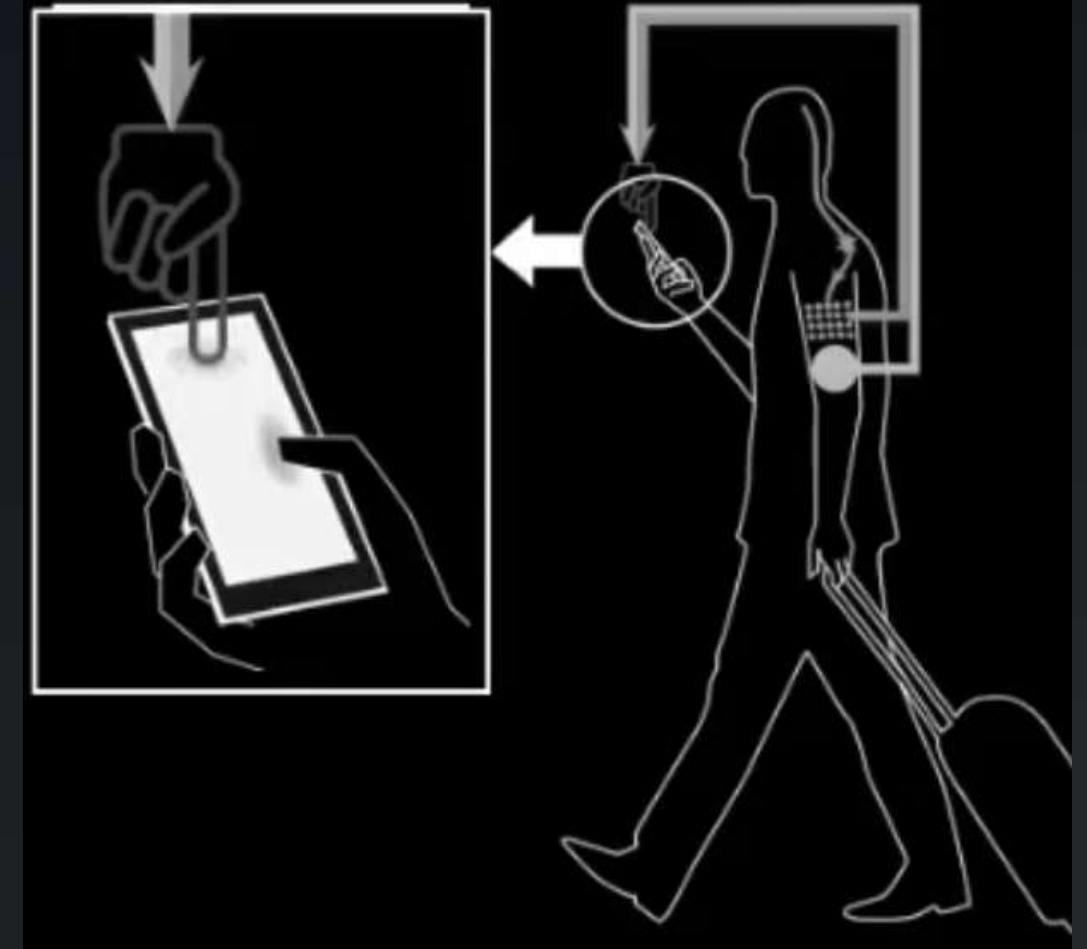
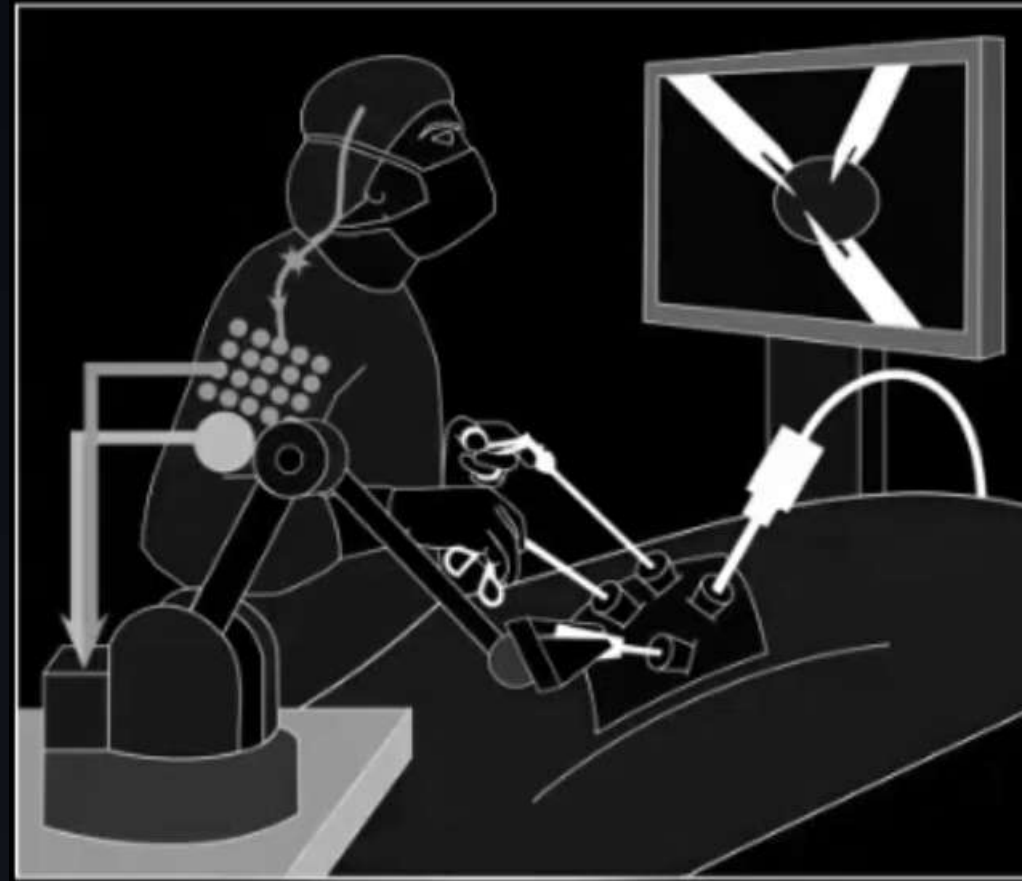
Autonomous



Whole-body

APPLICATIONS

- Medical Interventions
- Use of computers/mobile devices
- Paralysed patients with residual movement abilities
- Day-to-day activities e.g. playing an instrument



BIONICS



BIONIC HANDS AND ARMS IN PRINCIPLE CAN BE **STRONGER, FASTER** AND CAN **SENSE** WITH HIGHER ACCURACY THAN BIOLOGICAL ONES

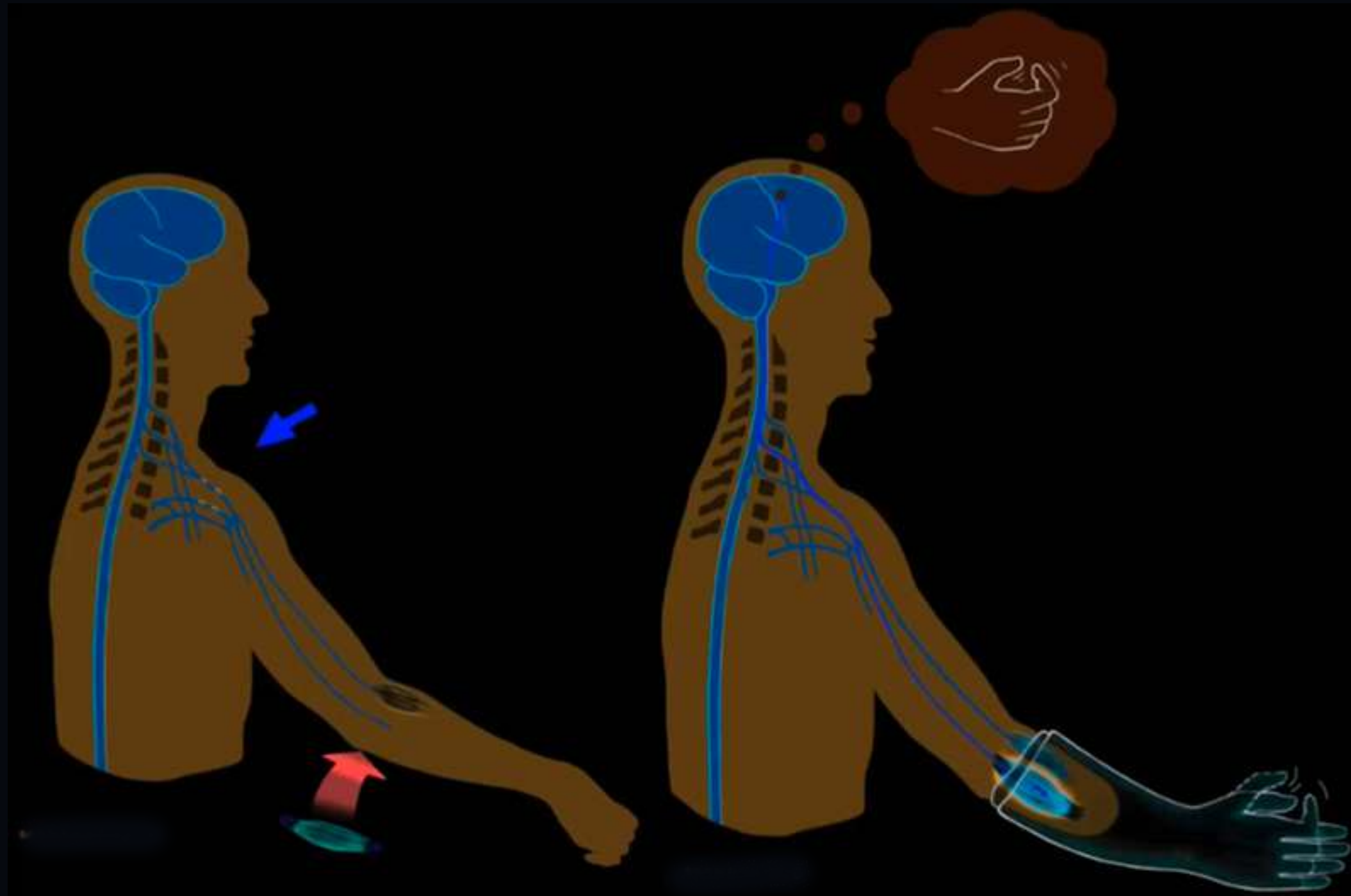


Open Bionics Hero Arm

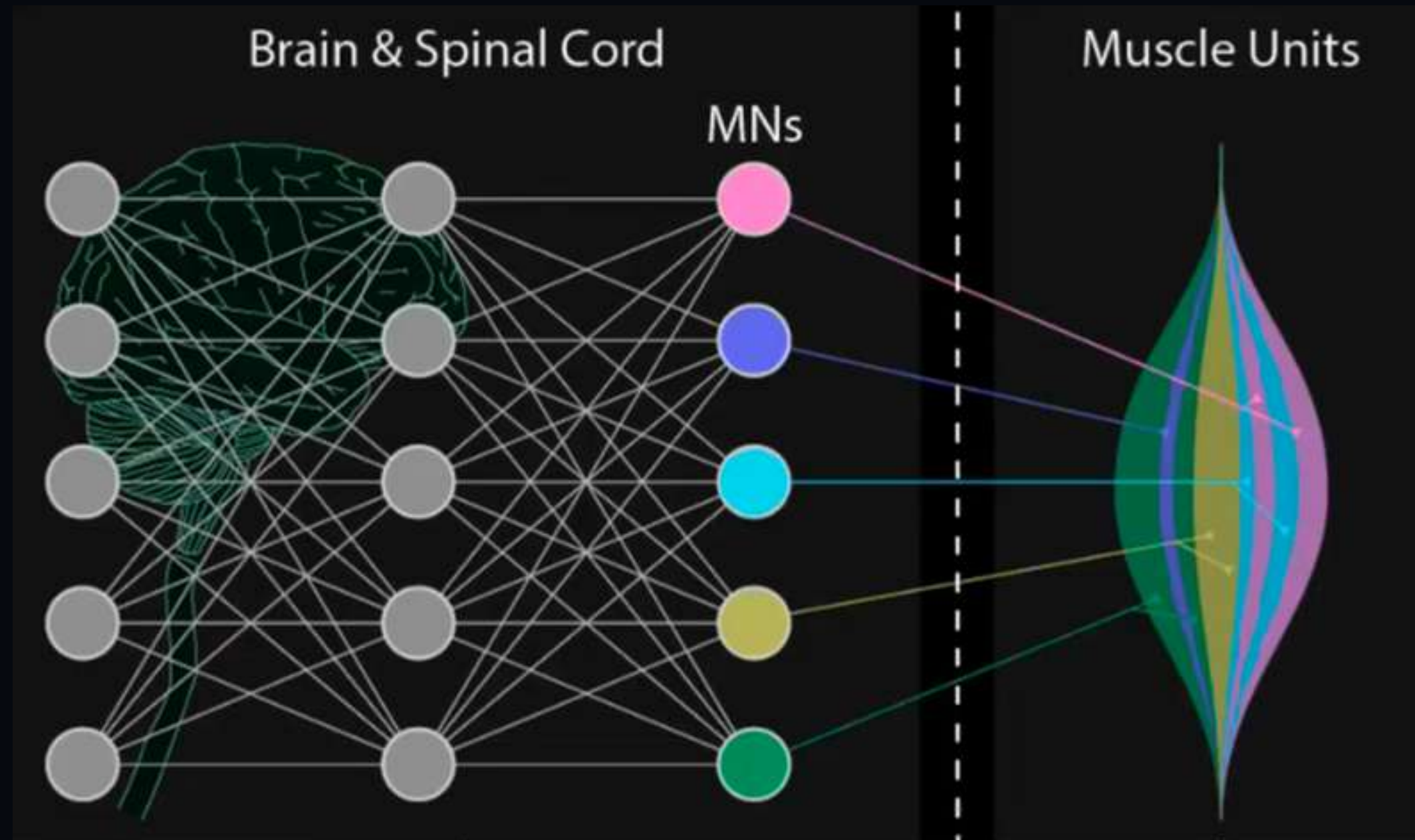
THE GAP BETWEEN AUTONOMOUS ROBOTS AND HUMAN-INTERFACED ROBOTS



CREATING AN **INTERFACE** AND REPLACING THE BIOLOGICAL HAND

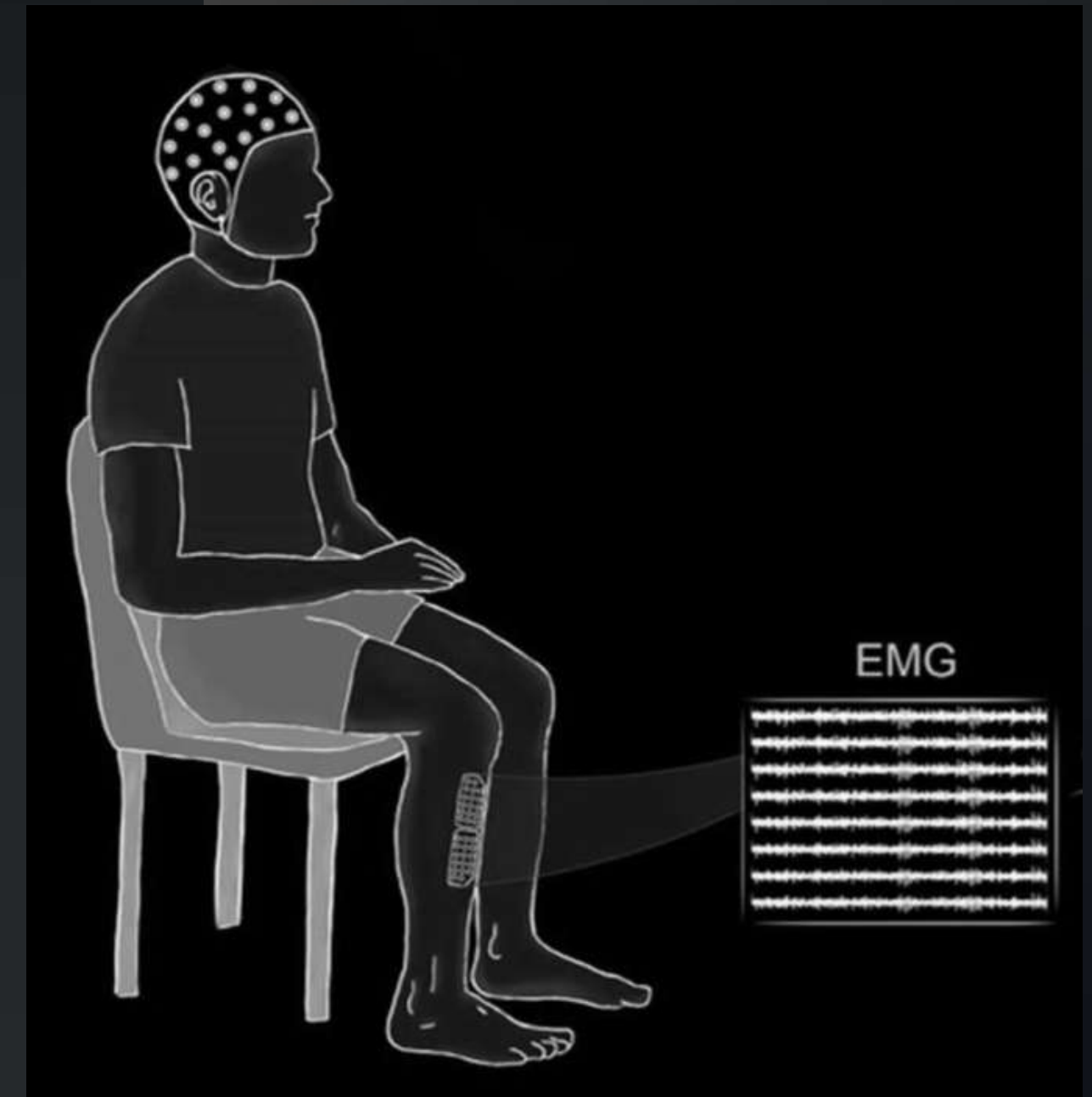


BIOLOGICALLY INSPIRED ARTIFICIAL CLASSIFIER NETWORK



METHODOLOGY: DATA COLLECTION

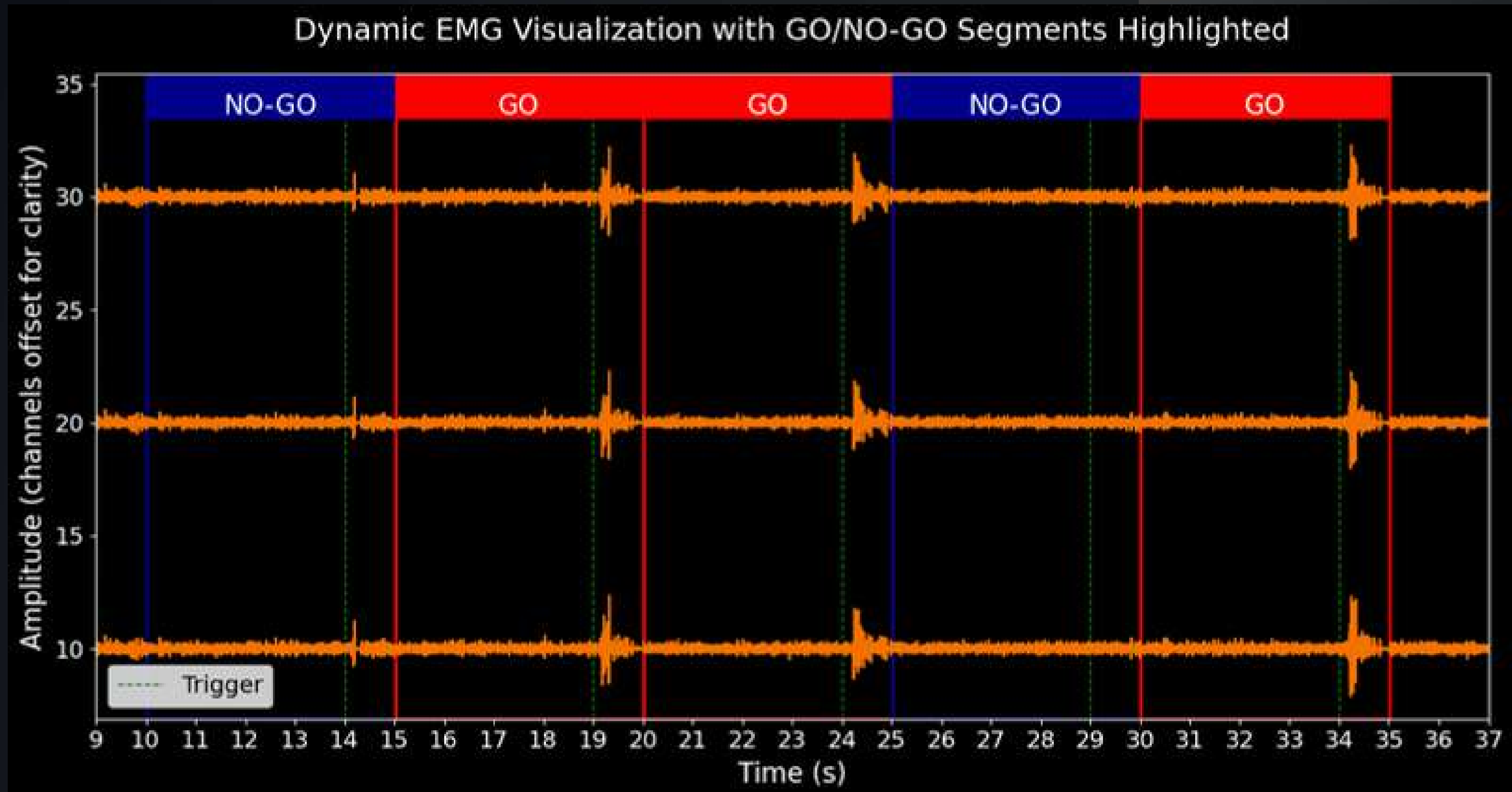
- **Overview:** The study examined neural input modulations during movement cancellation using a “GO/NO-GO” task.
- **Participants:** 12 male subjects (ages 21–38); ethical approval and consent obtained.
- **Setup:** EEG (31 electrodes) and high-density EMG (64 channels) recorded from the tibialis anterior muscle. Participants performed isometric ankle dorsiflexion at 10% MVC.
- **Task:** In “GO” trials, a ballistic contraction was performed. In “NO-GO” trials, force was maintained at 10% MVC. Each block had 35 trials, with fixed timing for auditory cues.



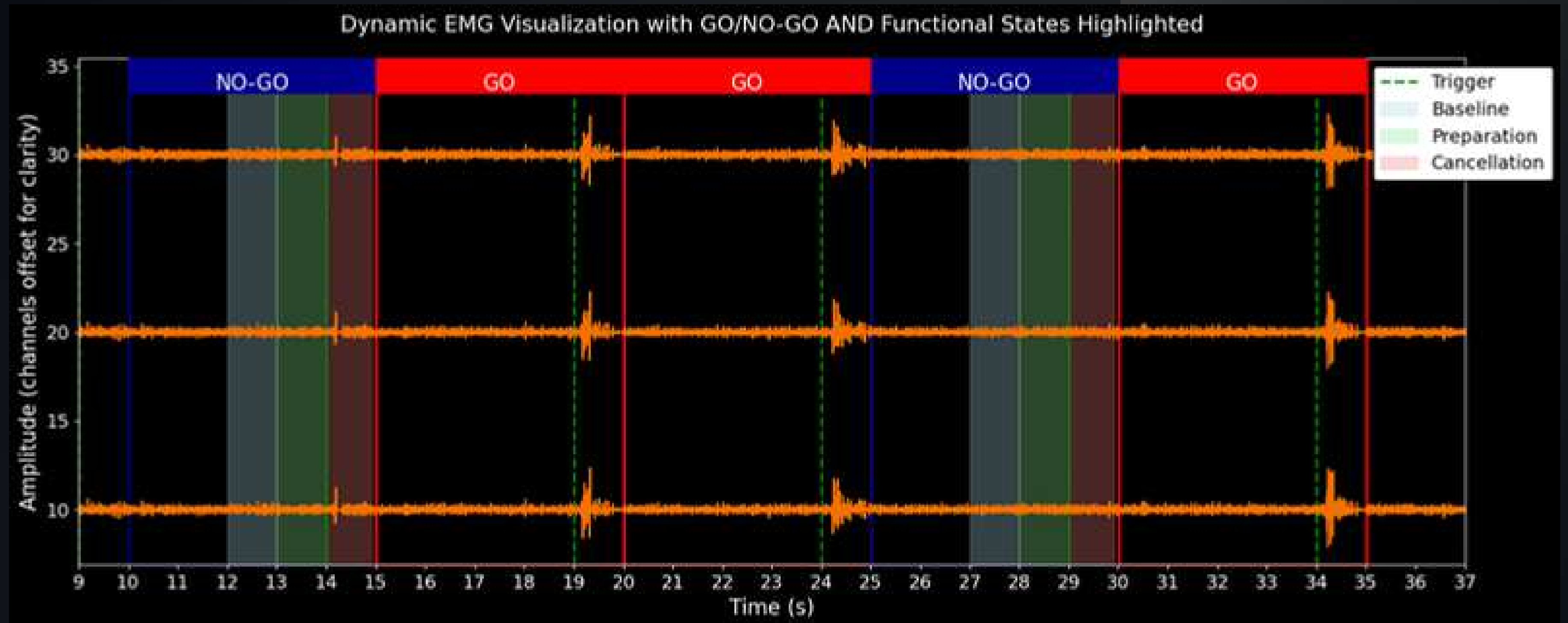
[2]

Zicher, B., et al. (2024). Journal of Neural Engineering, 21(056039).
<https://doi.org/10.1088/1741-2552/ad8835>

GO/NO-GO EXPERIMENT PARADIGM



FUNCTIONAL STATES



METHODOLOGY: DATA PREPROCESSING

INITIAL PIPELINE

Segment data

Select NO-GO regions
Extract Baseline,
Preparation and
Cancellation windows

Shape: Participant, Class,
no. of trials, samples,
channels
(7, 3, X, 2048, 64)

METHODOLOGY: DATA PREPROCESSING

INITIAL PIPELINE

Segment data

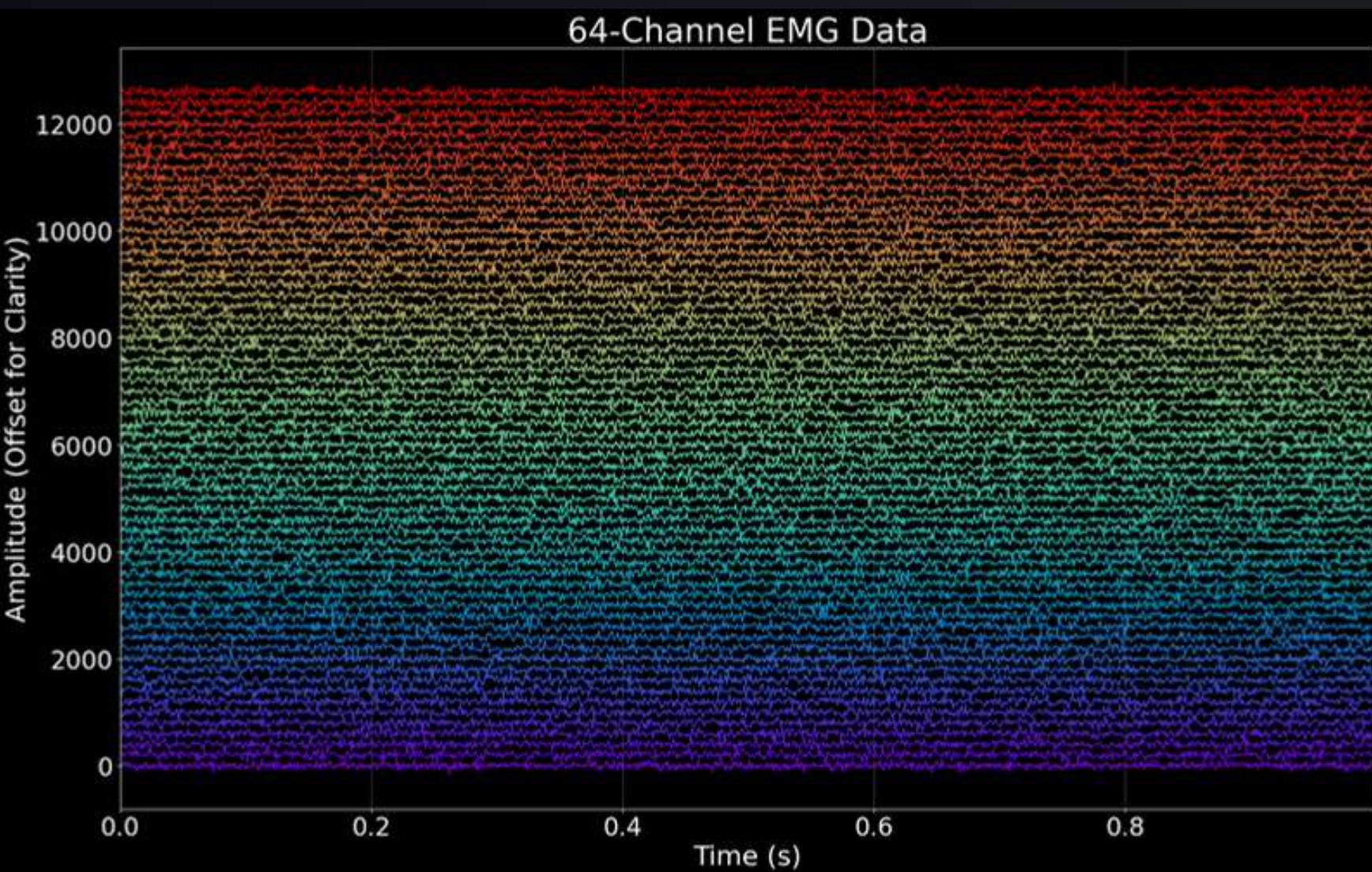
Select NO-GO regions
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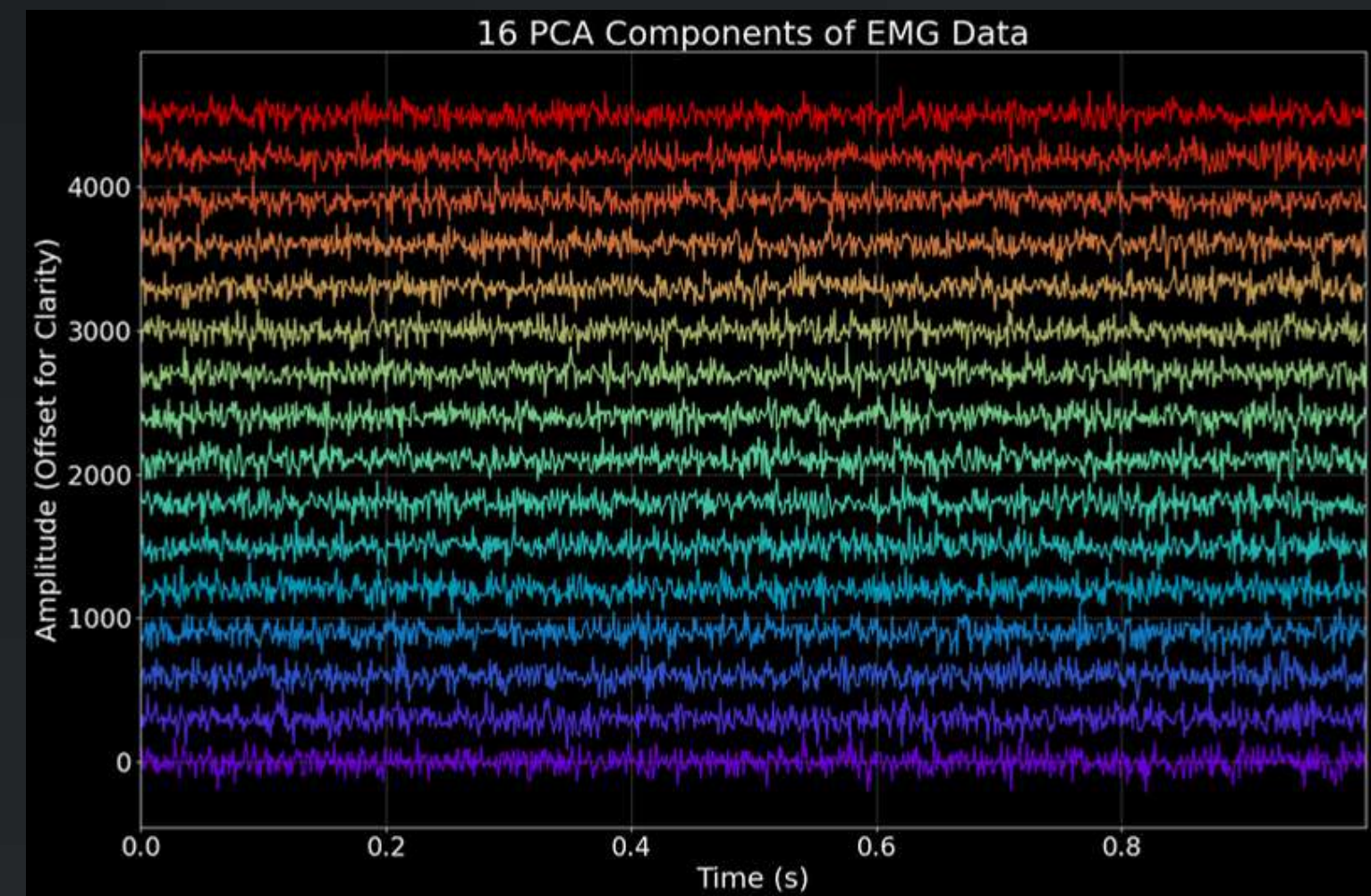
Channel Reduction through PCA

Shape: (7, 3, X, 2048, 16)

PRINCIPAL COMPONENT ANALYSIS



PCA
Reduction
→
64 Channel
EMG to 16 PCA
Components



METHODOLOGY: DATA PREPROCESSING

Segment data

Select NO-GO regions
Extract Baseline,
Preparation and
Cancellation windows

Shape: Participant, Class,
no. of trials, samples,
channels
(7, 3, X, 2048, 64)

Filtering and Normalisation

Bandpass
filtering (13-30Hz)

Downsample to 512Hz

Amplitude and Z-score
normalization

Shape:
(7, 3, X, 512, 16)

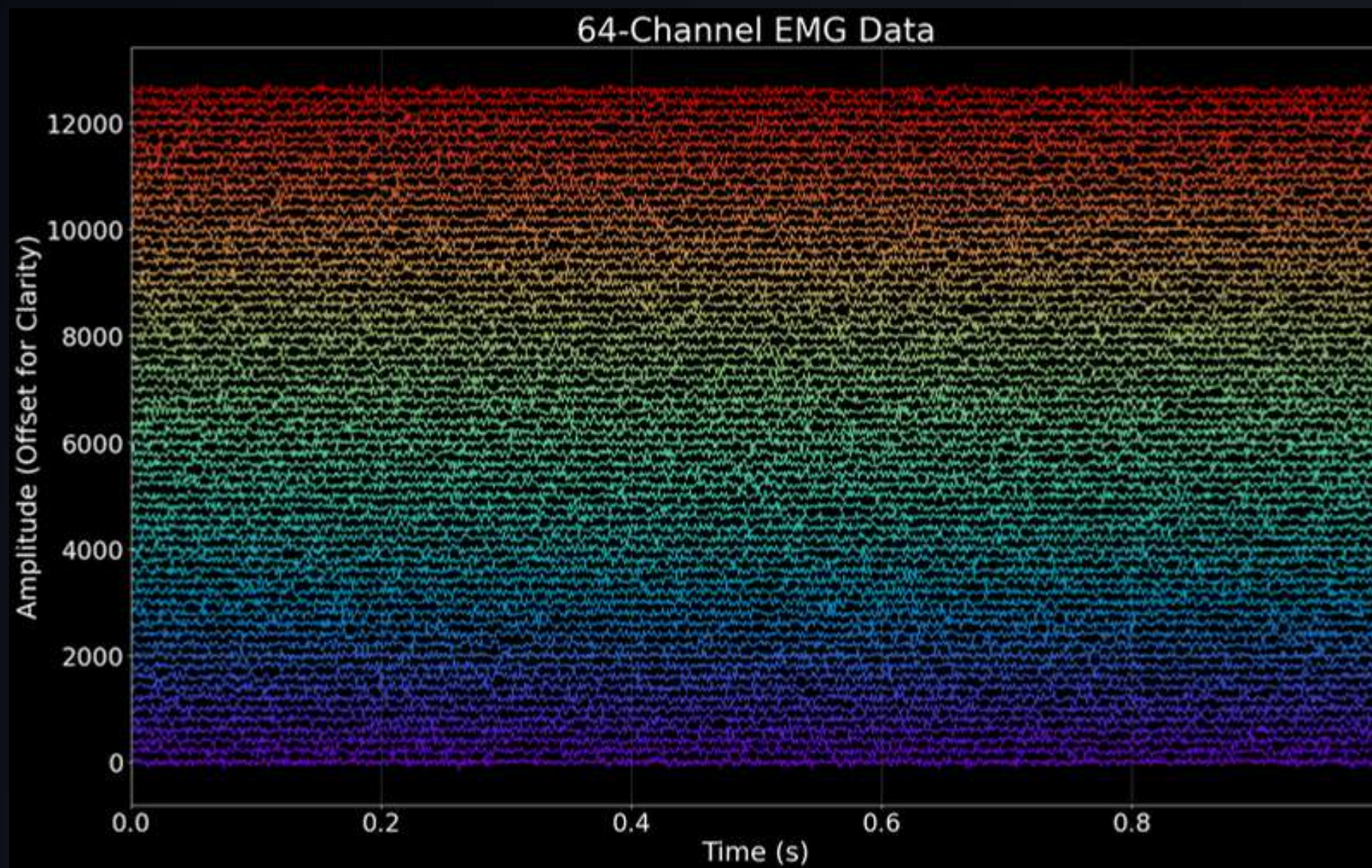
Channel Reduction through PCA

Shape: (7, 3, X, 2048, 16)

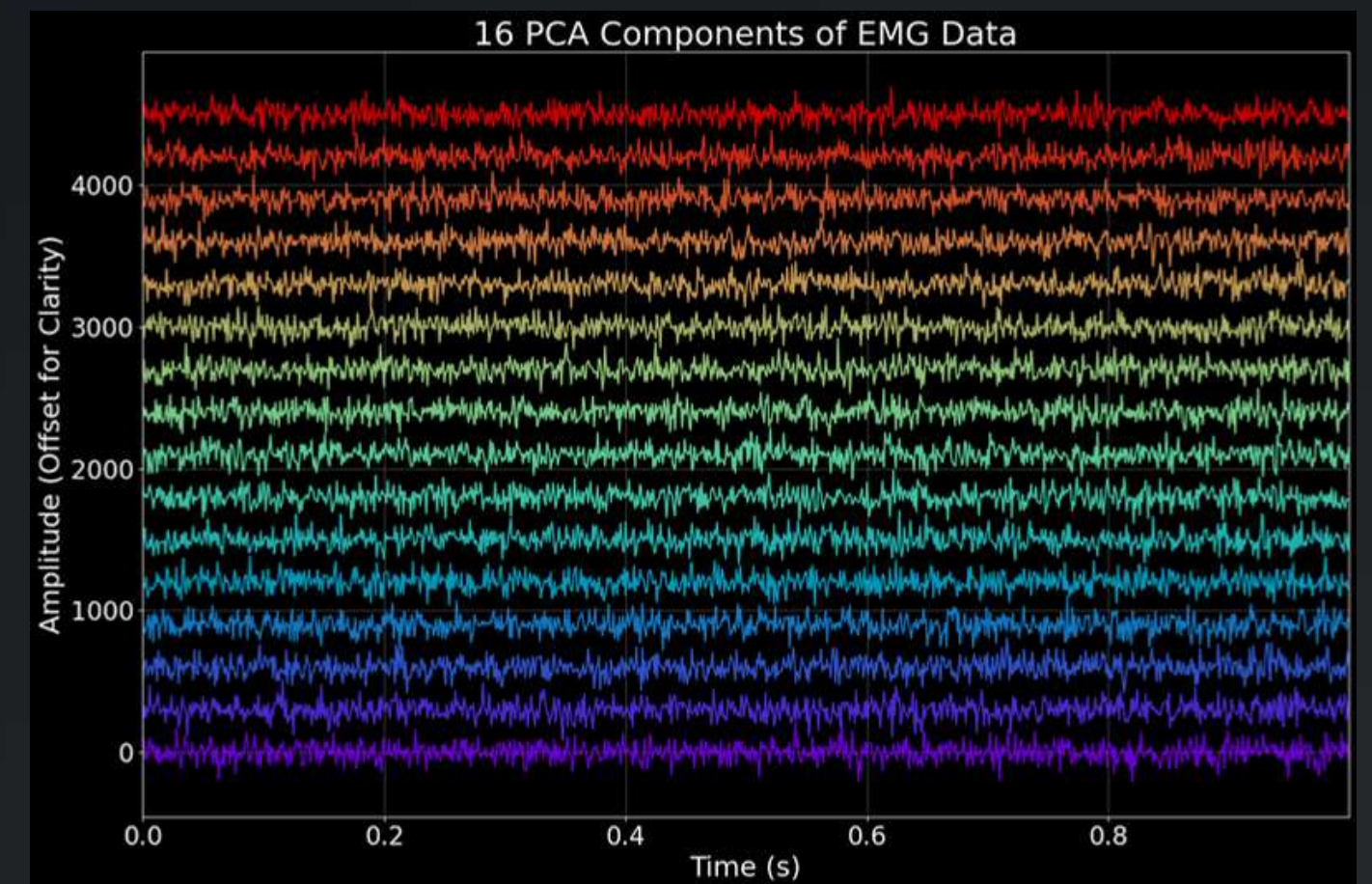
Data augmentation

Jittering and slight
augmentations to frequency
range of randomly selected
trials

Shape:
(7, 3, X, 512, 16)

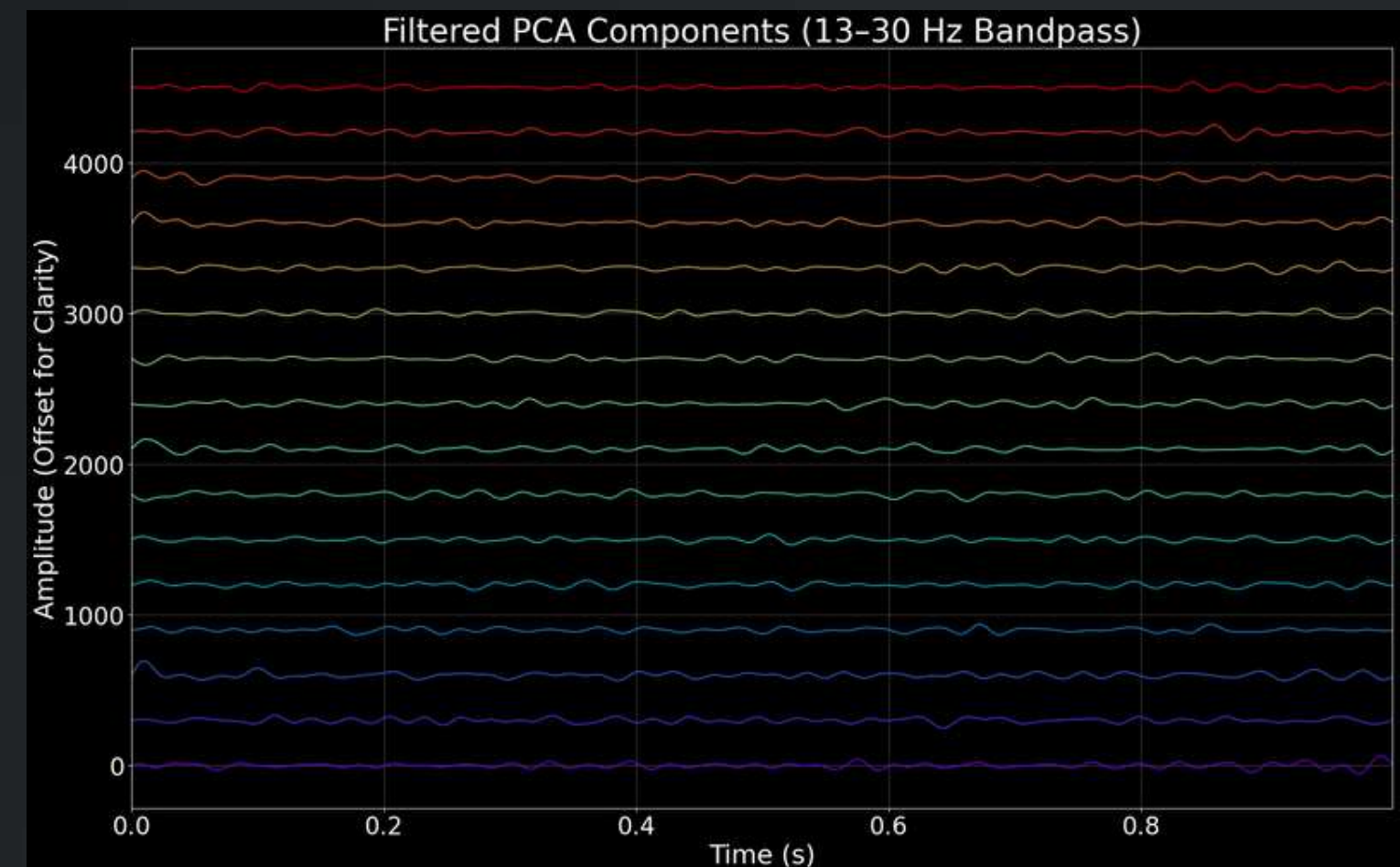


PCA
Reduction



FILTERING AND NORMALISATION

- Amplitude normalisation per trial
- Z-score normalization
- Data augmentation (jittering, slight augmentations to frequency filtering)



Beta Band
Bandpass
Filtering
(13-30Hz)

METHODOLOGY: DATA PREPROCESSING

Segment data

Select NO-GO regions
Extract Baseline,
Preparation and
Cancellation windows

Shape: Class, no. of trials,
samples, channels
(7, 3, X, 2048, 64)

Filtering and Normalisation

Bandpass
filtering (13-30Hz)

Downsample to 512Hz

Amplitude and Z-score
normalization

Shape:
(7, 3, X, 512, 16)

Beta Power

Compute Beta Power across
channels

Smooth beta power curves

Shape: (7, 3, X, 512, 1)

Channel Reduction through PCA

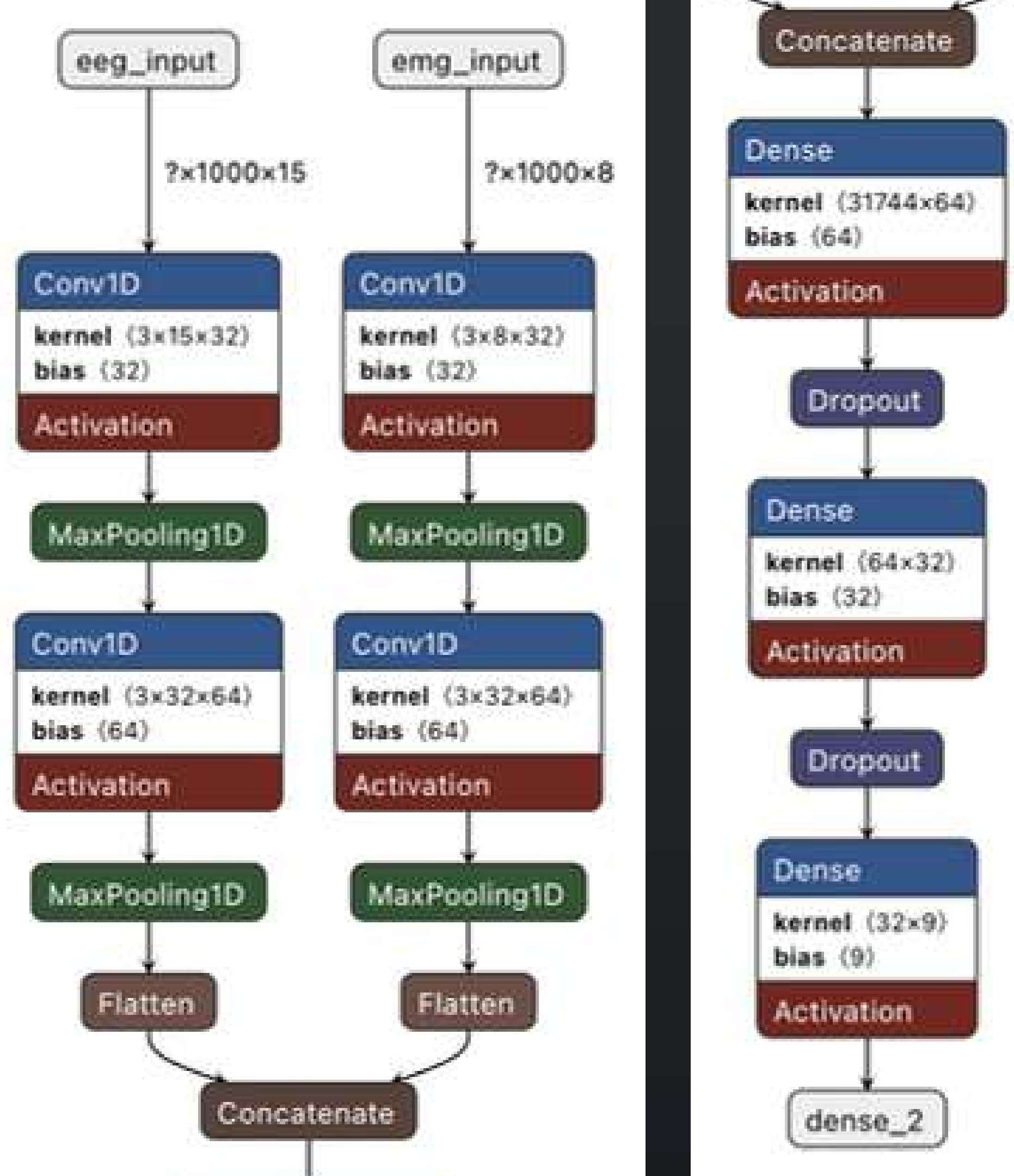
Shape: (7, 3, X, 2048, 16)

Data augmentation

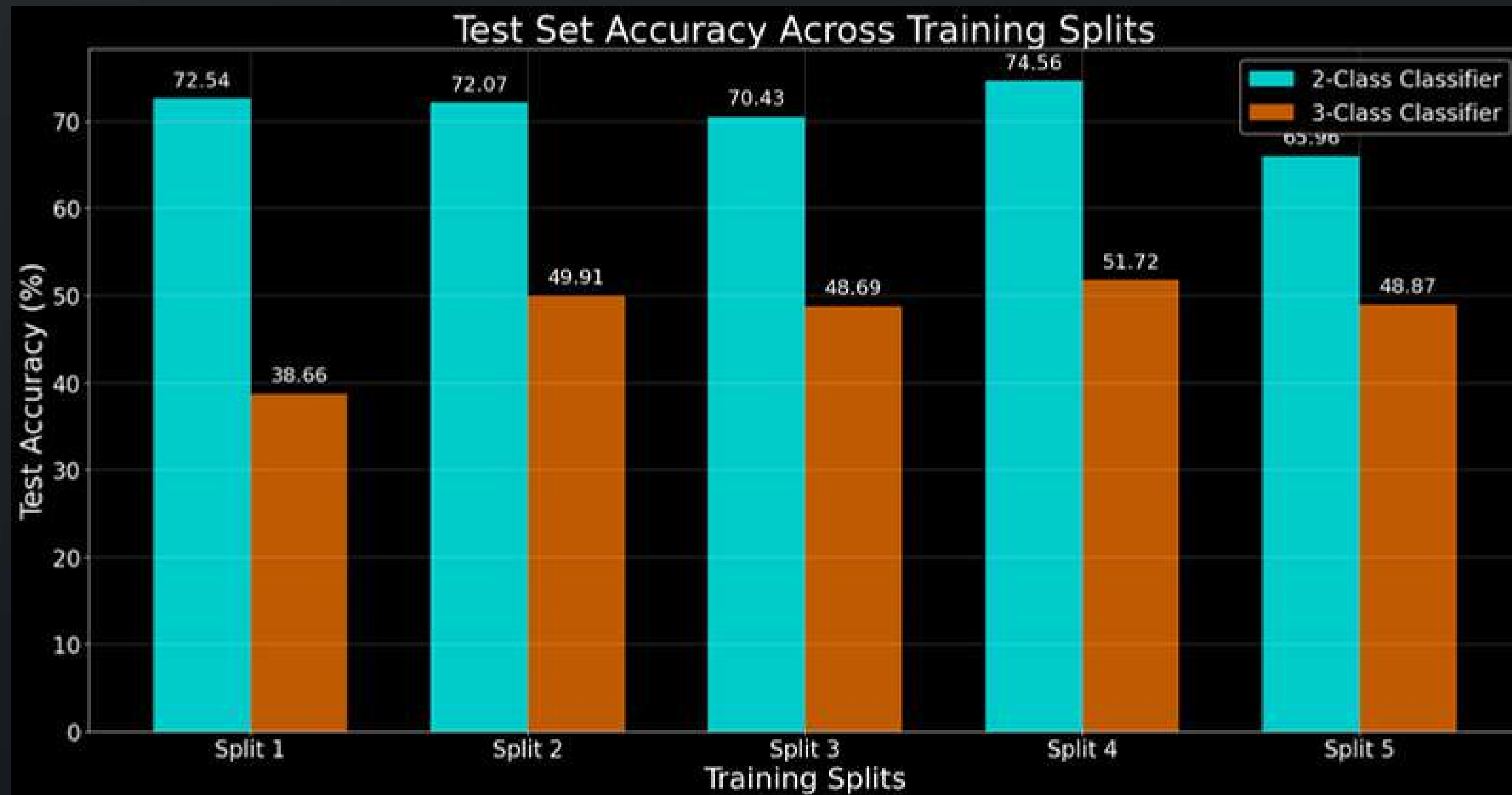
Jittering and slight
augmentations to frequency
range of randomly selected
trials

Shape: (7, 3, X, 512, 16)

METHODOLOGY: CLASSIFIER NETWORK



INITIAL RESULTS: ACCURACY



2-Class Average Accuracy: 72.4%

3-Class Average Accuracy: 49.6%

INITIAL RESULTS: LOSS



2-Class Average Loss: 0.532
3-Class Average Loss: 0.900

ANALYSIS: GRADCAM

Gradient-weighted Class Activation Mapping (GradCAM) is a visualization technique used to understand and interpret the decisions made by convolutional neural networks (CNNs).

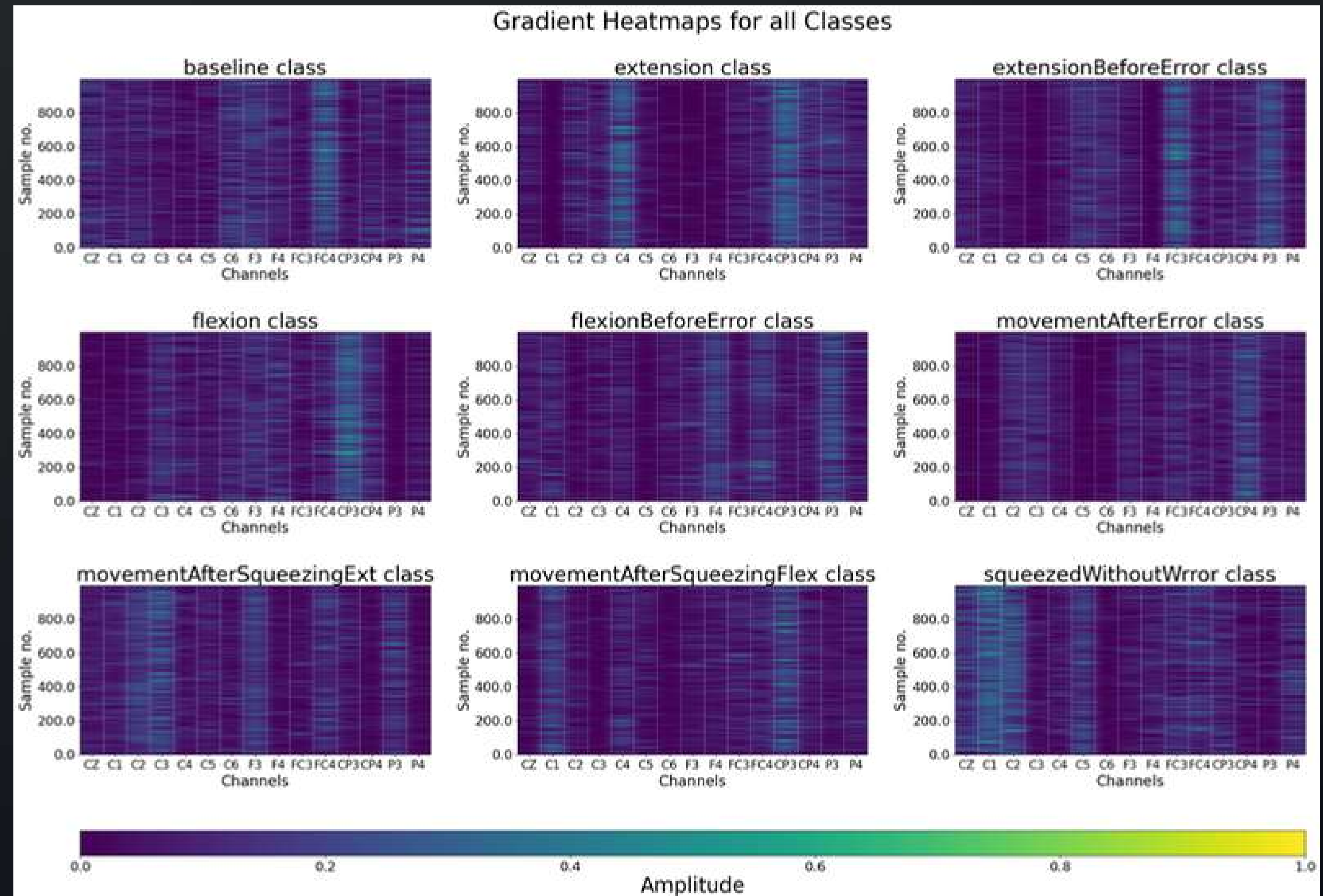
GradCAM highlights the regions in the input data that are most influential in predicting a particular class, providing insights into the model's decision-making process.

GradCAM works by computing the **gradient** of the predicted class score with respect to the activations of a convolutional layer. These gradients are then weighted by the average gradient across the spatial dimensions.



ANALYSIS: GRADCAM

Gradient Heatmap Visualization



CURRENT ADJUSTMENTS

Leverage Temporal Context

- Use the fact that the preparation class is always followed by cancellation.
- Explore merging “Preparation” and “Cancellation” classes into a single class.
- Perform comparisons:
 - Cancellation vs Baseline
 - Baseline vs Preparation + Cancellation
- Introduce a sliding window approach to capture dynamic changes.

Alternative Input Configurations

- Use all 64 channels directly as classifier input (bypass PCA).
- Calculate the mean of the square of the 64 channels as input instead of all individual channels.
- Evaluate classifier performance with and without PCA applied to the full set of 64 channels.
- Try calculating PCA across all trials collectively instead of per trial.

Ablation Studies

- Conduct stepwise ablations of preprocessing steps (e.g., filtering, normalization).
- Measure and compare classifier performance after removing or modifying specific steps.
- Present findings in a key or matrix format for clarity.

Alternative Techniques

- Apply KL Transform or Maximum Relevance Minimum Redundancy (mRMR) to evaluate feature selection efficacy.
- Compare results of KL Transform and mRMR techniques against PCA.

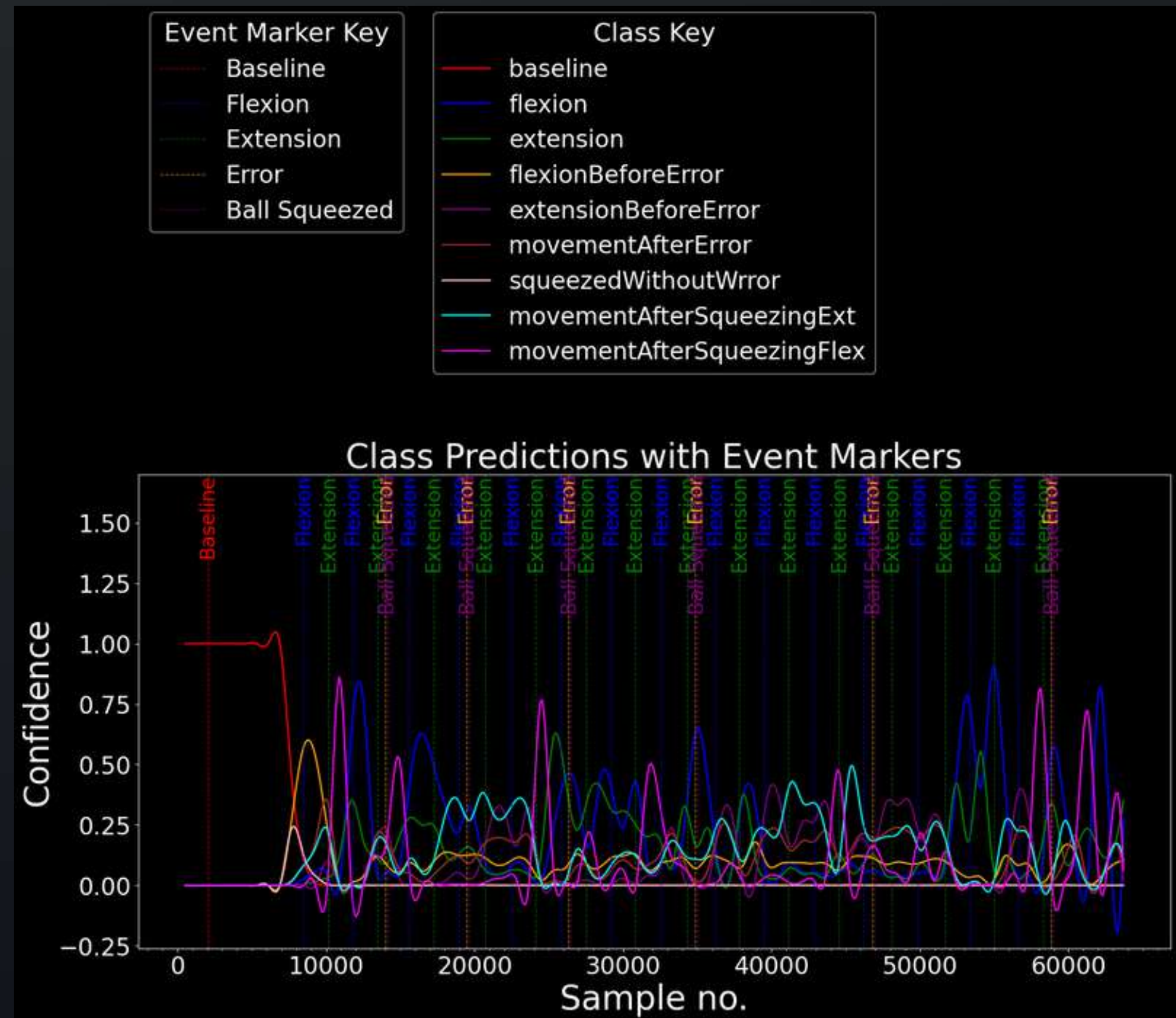


CLASSIFIER NETWORK: KEY CLASSES

Key	Label	Description
0	Baseline	Baseline - Baseline run without errors was also included to establish a control dataset.
1	Flexion	Flexion - Flexion run without errors
2	Extension	Extension - Extension run without errors
3	Flexion Before Error	Flexion before err - Flexion run up until error is introduced
4	Extension Before Error	Extension before err - Extension run up until error is introduced
5	Movement After Error	Movement After Error - Movement after error is detected where subject is preparing to execute movement (squeeze the ball)
6	Squeezed Without Error	Squeezed Without Error - run where participant squeezed the ball without mistake/without an error
7	Movement After Squeezing Extension	Movement After Squeezing Extension - participant resuming extension run after ball squeezed
8	Movement After Squeezing Flexion	Movement After Squeezing Flexion - participant resuming flexion run after ball squeezed

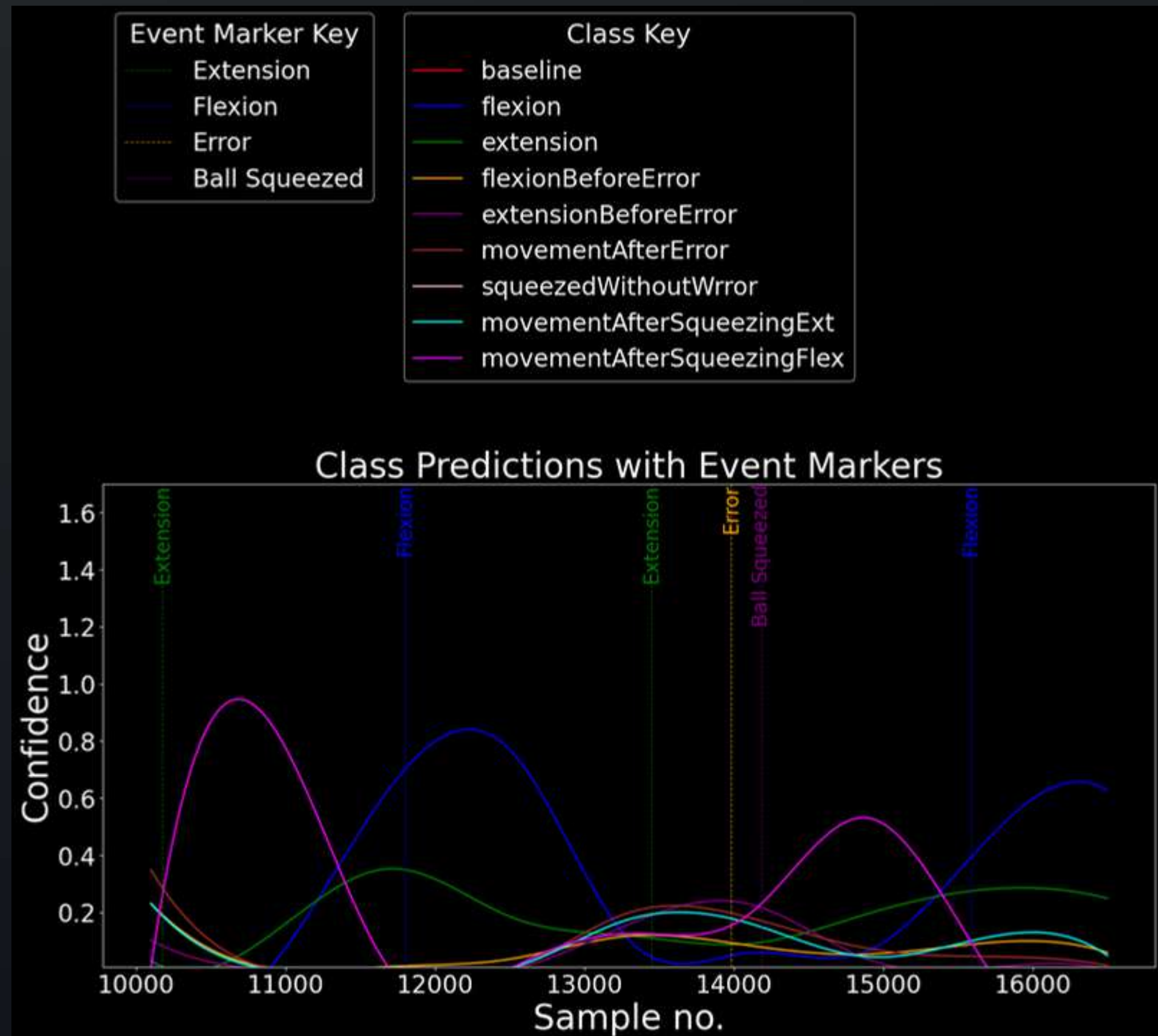
ANALYSIS: SLIDING WINDOW

Temporal Analysis
with Sliding
Window - **Overview**



ANALYSIS: SLIDING WINDOW

Temporal Analysis
with Sliding Window -
Detailed view

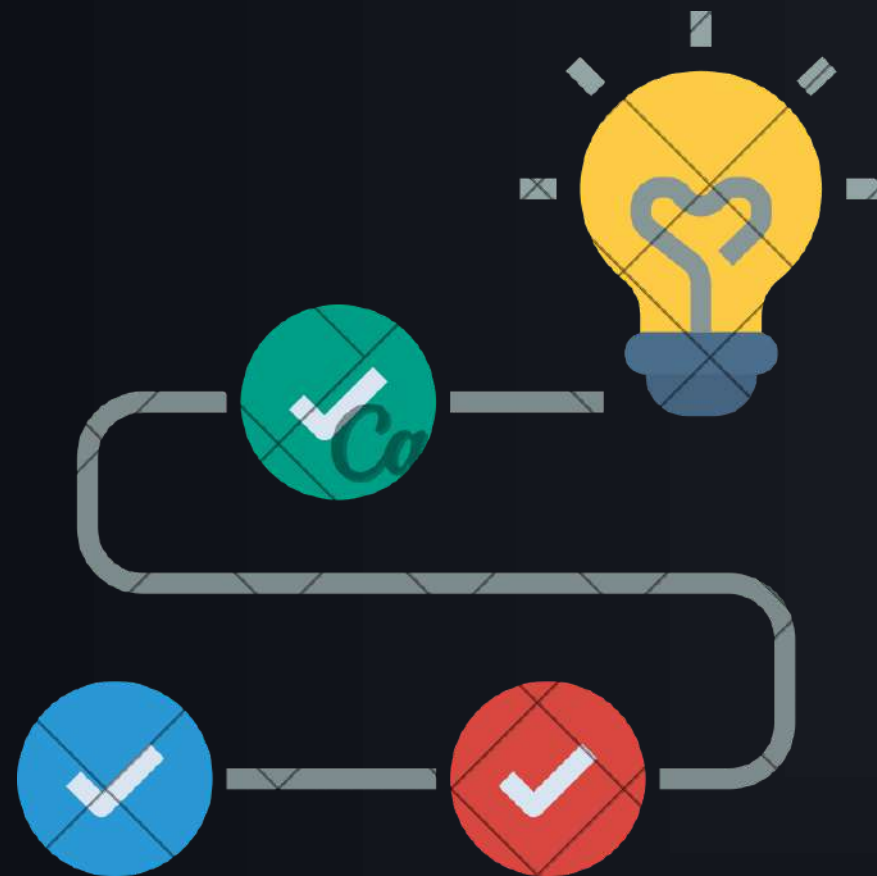


CONCLUSION

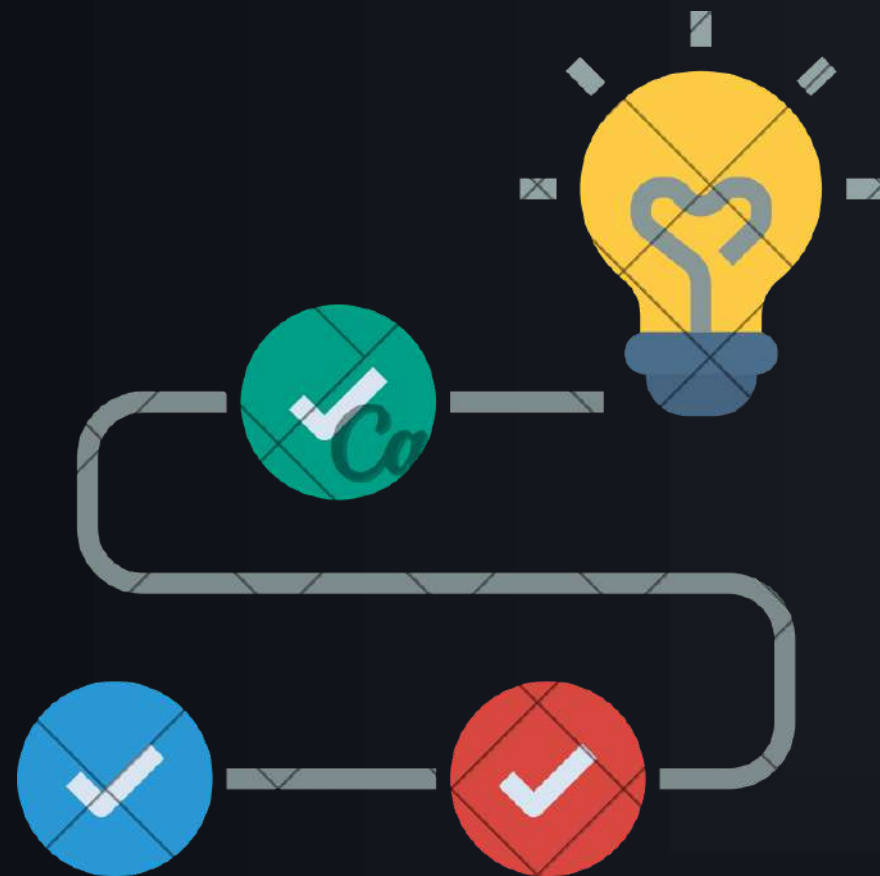
REVIEW

1

Our preliminary results have successfully demonstrated the feasibility of decoding central nervous system (CNS) activity using non-invasive electromyography (EMG) recordings.



CONCLUSION



REVIEW

1

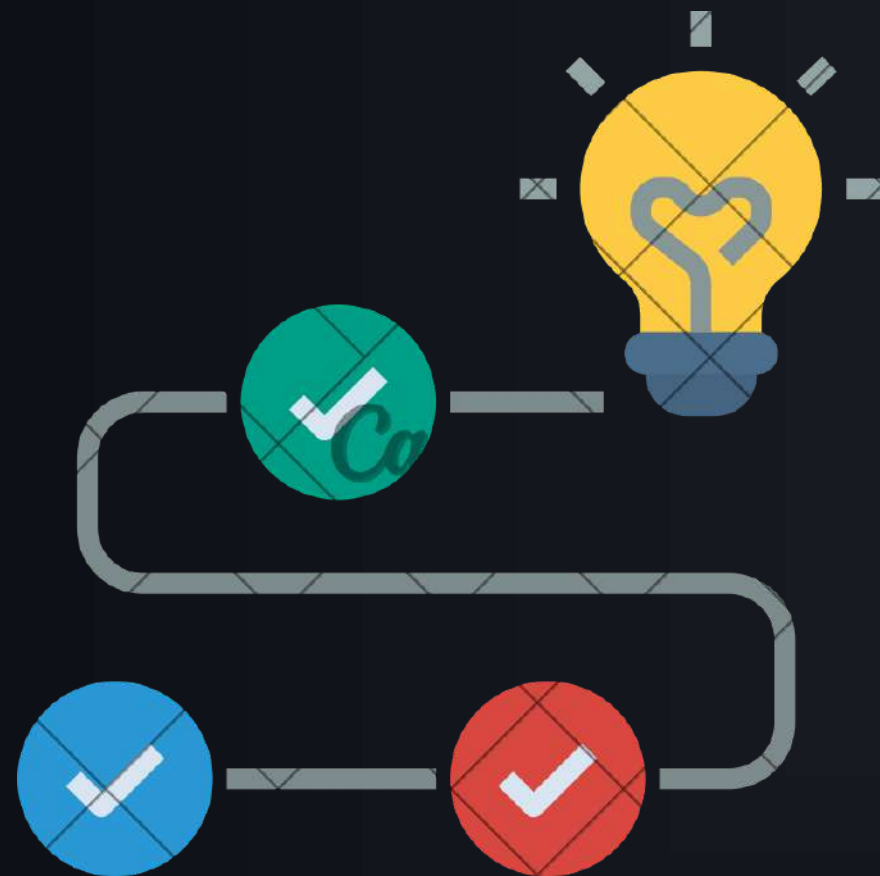
Our preliminary results have successfully demonstrated the feasibility of decoding central nervous system (CNS) activity using non-invasive electromyography (EMG) recordings.

IMPLICATIONS

2

The findings from this study have significant implications for various fields, including rehabilitation, prosthetics, and the broader field of neurotechnology, offering new insights into neural control mechanisms and paving the way for innovative human-machine interfaces (HMIs).

CONCLUSION



REVIEW

1

Our preliminary results have successfully demonstrated the feasibility of decoding central nervous system (CNS) activity using non-invasive electromyography (EMG) recordings.

IMPLICATIONS

2

The findings from this study have significant implications for various fields, including rehabilitation, prosthetics, and the broader field of neurotechnology, offering new insights into neural control mechanisms and paving the way for innovative human-machine interfaces (HMIs).

FUTURE WORK

3

I will focus on refining the AI model to enhance its accuracy and robustness. To build on our current results, I will devise specific experiments aimed at exploiting the full potential of EMG-based CNS decoding for HMI advancements in Real Time scenarios.

THANK YOU

QUESTIONS